less than the diameter of the wire making up the bare stent 30. Preferably, the space is no greater than half a diameter of the wire

Having the distal surface 639 be the load-bearing surface of the proximal apices 32 ensures expansion of each and every- 5 one of the distal apices 32 from the apex release assembly 690. The proximal surface 641 of the distal apex head 636 (see FIG. 30) meets with the interior surfaces of the proximal apex body 638 to help carry the apex load because the apices of the bare stent 30 are captured therebetween when the apex 10 capture device 634 is closed. Complete capture of the bare stent 30, therefore, fully transmits any longitudinal forces acting on the bare stent 30 to both the guidewire lumen 620 and apex release lumen 640, making the assembly much stronger. Such capture can be clearly seen in the cut-away 15 view of the proximal apex body 638 in FIG. 31. For release of the apices 32 of the bare stent 30, the proximal apex body 638 moves leftward with respect to FIGS. 30 to 33 (compare FIGS. 30 and 31 with FIG. 32). Because friction exists between the apices 32 and the "teeth" of the proximal apex 20 body 638 when the apices 32 are captured, the apices 32 will also try to move to the left along with the proximal apex body 638 and, if allowed to do so, possibly would never clear the "teeth" to allow each apex 32 to expand. However, as the proximal apex body 638 disengages (moves in the direction 25 of arrow C in FIG. 31), direct contact with the distal surface 639 entirely prevents the apices 32 from sliding in the direction of arrow C along with the proximal apex body 638 to ensure automatic release of every captured apex 32 of the bare stent 30. Because the proximal apex body 638 continues to 30 move in the direction of arrow C, eventually the "teeth" will clear their respective capture of the apices 32 and the bare stent 30 will expand entirely. The release position of the distal apex head 636 and the proximal apex body 638 is shown in FIGS. 14 and 32, and corresponds to the position of the apex 35 release assembly 690 in FIG. 17. As can be seen, tapers on the distal outer surfaces of the proximal apex body 638 further assist in the prevention of catching the proximal apices 32 of the bare stent 30 on any part of the apex capture device 634. In this configuration, the distal surfaces 639 bear all the load 40 upon the bare stent 30 and the fingers of the proximal apex body 638.

Simply put, the apex capture device 634 provides support for load placed on the stent graft 1 during advancement A of the inner sheath 652 and during withdrawal of the inner 45 sheath 652 (i.e., during deployment D). Such a configuration benefits the apposition of the bare stent 30 by releasing the bare stent 30 after the entire graft sleeve 10 has been deployed, thus reducing the potential for vessel perforation at the point of initial deployment.

When the stent graft 1 is entirely free from the inner sheath 652 as shown in FIG. 24, the proximal handle 678 is, then, substantially at or near the third position (deployment position) shown in FIG. 10.

The stent graft 1 is, now, securely placed within the vessel 700 and the entire portion 630, 650, 660 of the assembly 600 may be removed from the patient.

While the preferred embodiments of the invention have been illustrated and described, it will be clear that the invention is not so limited. Numerous modifications, changes, variations, substitutions, and equivalents will occur to those skilled in the art without departing from the spirit and scope of the present invention as defined by the appended claims.

What is claimed is:

- 1. A method of implanting a prosthesis in a patient at a treatment site within a blood vessel, comprising the steps of:
- a) advancing an outer catheter of a prosthesis delivery system in the patient distal to the treatment site, the outer catheter defining an inside diameter and wherein the treatment site is a curved portion of the aortic arch;
- b) advancing an inner sheath containing a prosthesis that is asymmetric about a major longitudinal axis, the inner sheath having greater flexibility than the outer catheter and an outside diameter that is greater than the inside diameter of the outer catheter, and a guidewire lumen of the delivery system from the outer catheter and then through the curved portion of the aortic arch along a guidewire while the outer catheter remains stationary relative to the patient, whereby advancement of the inner sheath and the guidewire lumen delivers the prosthesis to a position within the curved portion of the aortic arch and causes rotational alignment of the prosthesis within the curved portion of the aortic arch;
- c) retracting the inner sheath to deploy the prosthesis from within the inner sheath at the curved portion of the aortic arch; and
- d) retracting the delivery system from the patient.
- 2. The method of claim 1, further comprising the step of retracting the inner sheath into the outer catheter prior to retracting the delivery system from the patient.
- 3. The method of claim 1, wherein the guidewire lumen is curved.
- 4. The method of claim 1, wherein the prosthesis includes a longitudinal support member positioned asymmetrically about the major longitudinal axis of the prosthesis to thereby cause the rotational alignment within the curved portion of the aortic arch.

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